Obstructive sleep apnea in older adults is a distinctly different physiological phenotype

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Obstructive Sleep Apnea in Older Adults is a Distinctly Different Physiological Phenotype

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Study Objectives: Current evidence suggests that the pathological mechanisms underlying obstructive sleep apnea (OSA) are altered with age. However, previous studies examining individual physiological traits known to contribute to OSA pathogenesis have been assessed in isolation, primarily in healthy individuals.

Design: We assessed the four physiological traits responsible for OSA in a group of young and old patients with OSA.

Setting: Sleep research laboratory.

Participants: Ten young (20-40 y) and old (60 y and older) patients with OSA matched by body mass index and sex.

Measurements and Results: Pharyngeal anatomy/ collapsibility, loop gain (LG), upper airway muscle responsiveness/gain (UAG) and the respiratory arousal threshold were determined using multiple 2- to 3-min decreases or drops in continuous positive airway pressure (CPAP). Passive pharyngeal anatomy/collapsibility was quantified as the ventilation at CPAP = 0 cmH2O immediately after the CPAP drop. LG was defined as the ratio of the ventilatory overshoot to the preceding reduction in ventilation. UAG was taken as the ratio of the increase in ventilation to the increase in ventilatory drive across the pressure drop. Arousal threshold was estimated as the ventilatory drive that caused arousal. \( V_{\text{eupnea}} \) was quantified as the mean ventilation prior to the pressure drop. In comparison with younger patients with OSA, older patients had a more collapsible airway (ventilation at 0 cmH2O = 3.4 ± 0.9 versus 1.5 ± 0.7 L/min; \( P < 0.05 \)) but lower \( V_{\text{eupnea}} \) (8.2 ± 0.5 versus 6.1 ± 0.4 L/min; \( P < 0.01 \)) and a lower LG (5.0 ± 0.7 versus 2.9 ± 0.5; \( P < 0.05 \)). The remaining traits were similar between groups.

Conclusions: Our data suggest that airway anatomy/ collapsibility plays a relatively greater pathogenic role in older adults, whereas a sensitive ventilatory control system is a more prominent trait in younger adults with obstructive sleep apnea.

Keywords: aging, loop gain, lung, obstructive sleep apnea, sleep disordered breathing, upper airway collapsibility

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INTRODUCTION

Obstructive sleep apnea (OSA) is a common disorder characterized by repetitive collapse or obstruction of the pharyngeal airway during sleep.\(^1\) The resultant hypoxemia/hypercapnia, sympathetic activation, and sleep disruption often lead to impaired neurocognitive function and excessive daytime sleepiness.\(^2\) Furthermore, patients with OSA are at higher risk of cardiovascular diseases, including hypertension, myocardial infarction, stroke, and heart failure, making it a major health problem.\(^3,4\)

Aging is known to be an important factor contributing to the risk of OSA, with rising disease prevalence across a wide spectrum of ages.\(^5\) Of note, a recent large study demonstrated that 50% of older men had a respiratory disturbance index > 13/h, with aging being an independent risk factor in multivariate analysis.\(^6\) In some but not all studies, OSA is a cause of increased mortality in older adults, with one large study demonstrating that patients older than 70 y with severe OSA have a significantly shorter survival time.\(^7\) However, the mechanisms whereby aging increases the risk of OSA are not completely understood. OSA occurrence with aging may be driven by one or more of the physiological characteristics known to be important in OSA pathogenesis, with four of the most recognized factors being a poor upper airway anatomy (i.e., a highly collapsible airway), ineffective upper airway dilator muscle activity/responsiveness, a low respiratory arousal threshold, or an unstable ventilatory control system.\(^8,10\)

Prior studies, limited primarily to healthy individuals (i.e., without OSA), have suggested that upper airway collapsibility worsens with age\(^11,12\) and that the ventilatory control system becomes more stable.\(^13\) Furthermore, older subjects tend to have an increased frequency of spontaneous arousals\(^14\) (i.e., suggestive of a lower arousal threshold) and reduced upper airway muscle reflex response to negative pressure\(^15\) in comparison with their younger counterparts. Collectively, these changes with aging in healthy individuals suggest that OSA might be caused by different mechanisms in older versus younger individuals. Since previous studies examined individual physiological traits in isolation, mainly in healthy individuals, this concept has not been adequately investigated. Accordingly, using a recently validated technique,\(^16\) the current study aims to investigate the effect of aging on four key traits responsible for OSA in a group of young and older patients with OSA. Preliminary results of this analysis have been published in abstract form.\(^16\)
METHODS

Participants

Ten relatively young (20-40 y) and ten older (60 y and older) body mass index (BMI) and sex-matched (matched on group means) patients with OSA were recruited from our sleep clinic. All subjects had a history of OSA with an apnea/hypopnea index (AHI) > 10 events/h during supine non-rapid eye movement (NREM) sleep and were treated with continuous positive airway pressure (CPAP) for more than 5 h per night for at least 2 mo prior to enrollment. Written, informed consent was given before participation in the study, which was approved by the Human Research Committee at Brigham and Women’s Hospital. Subjects were excluded if they had a history of renal failure, neuromuscular disease or other major neurological disorders, uncontrolled diabetes, heart failure, central sleep apnea/Cheyne-Stokes respiration, uncontrolled hypertension, thyroid disease, or any other unstable medical condition. Female subjects were also screened to ensure that they were not pregnant. Of the young subjects, one was on a medication to lower cholesterol and another was taking an antihypertensive medication. In the elderly subjects, three subjects were receiving antihypertensive medications, two were on medications to lower cholesterol, two were on medications to treat arthritis, and one was taking medications for gastroesophageal reflux disease and depression. An important consideration in our experimental design was whether to study patients who are untreated or patients who are currently treated with CPAP therapy; several studies\textsuperscript{17,18} have recently demonstrated that some of the phenotypic traits are altered as a consequence of disease and that studying compliant CPAP users (after at least 1 mo of therapy) allows a patient’s intrinsic physiology to be determined. As the aim of the study was to examine changes in the intrinsic physiological traits with age rather than the degree to which the traits are affected by OSA per se and its progression, we studied patients who were CPAP compliant.

Experimental Design and Protocol

Each subject underwent a clinical polysomnogram (PSG) to measure OSA severity and a research PSG to measure the four OSA traits. For the clinical PSG, subjects were set up with the standard clinical montage that included electroencephalogram (EEG), electrooculogram, submental and leg electromyogram, electrocardiogram, nasal pressure and thermistor, respiratory effort (piezoelectric bands placed around the chest and abdomen), body position, and arterial oxygen saturation monitored at the finger. Subjects slept in the supine position for at least 4 h. All PSG data were collected and stored using the Alice digital PSG system (Philips Respironics, Murrysville, PA). A single sleep technician blinded to the subjects’ ages was responsible for scoring sleep state, arousals, and respiratory events according to standard American Academy of Sleep Medicine (AASM) criteria.\textsuperscript{19}

For the research PSG, subjects slept in the supine position with the same monitoring equipment as the clinical PSG. In addition, they were fitted with a sealed nasal mask (Gel Mask; Philips Respironics) attached to a pneumotachometer (model 3700A; Hans-Rudolph, Kansas City, MO) for measuring airflow. The mask was connected to a positive/negative pressure source (Perit 3000, Philips Respironics) to enable rapid switching between CPAP levels. The pressure in the mask was measured by a pressure transducer (Validyne, Northridge, CA) connected to a port in the mask. Carbon dioxide (CO\textsubscript{2}) was continuously recorded from a catheter placed inside the nostril and measured with a capnograph (Vacumed, Ventura CA). All signals were sampled at 125 Hz and displayed using Nihon Kohden (Tokyo, Japan) and Spike 2 software (Cambridge Electronic Design Ltd, Cambridge, UK).

Measuring the Traits Responsible for OSA

All subjects were initially placed on a level of CPAP that abolished flow limitation and snoring, with flow limitation defined as a characteristic peak–plateau or obvious flattening in inspiratory airflow. The method for measuring the physiological traits uses 2- to 3-min CPAP decreases or drops, repeatedly performed to varying degrees of sub-therapeutic pressures during stable NREM (i.e., stages 2-4) sleep (Figure 1), to produce differing degrees of flow limitation.\textsuperscript{8} The changes in ventilation that accompany the flow limitation are then used to calculate the four traits. The analysis of the data derived from the CPAP drop technique has been described in detail previously.\textsuperscript{8} Briefly, all artefact-free CPAP drops were imported into MATLAB (Mathworks, Natick, MA) for analysis. Tidal volume, breath duration, and breath-by-breath minute ventilation were calculated using the leak-corrected flow signal. CPAP drops were included only from periods when the subject was in the supine position.

Resting Ventilation

Before every CPAP drop, each subject’s resting minute ventilation (referred to as $V_{\text{eup}}$) was quantified as the mean ventilation 1 min prior to each CPAP drop.

Loop Gain, Delay, and the Time Constant

Loop gain (LG) is the ventilatory response to the disturbance ratio and is a measure of the sensitivity of the ventilatory control feedback loop. Figure 1 illustrates how LG can be measured from a CPAP drop. When CPAP is dropped, partial obstruction of the airway and a reduction in ventilation occur. Subsequently, carbon dioxide increases, which in turn increases ventilatory drive and stimulates upper airway muscle activation. The activation of these muscles can, in some patients, partially reopen the airway, and increase ventilation from the beginning of the CPAP drop to the end of the CPAP drop (defined by $V_{\text{eup}}$ in Figure 1). Despite this partial recovery, ventilation often remains below the eupneic level despite the increased levels of ventilatory drive. The amount that ventilatory drive rises over the course of the drop can be determined by returning CPAP to the therapeutic level (thereby rapidly opening the airway) and measuring the overshoot in ventilation ($V_{\text{p}}$). The ratio of this ventilatory response (labeled $V_{\text{r}}$) to the reduction in ventilation (ventilatory disturbance or $V_{\text{d}}$) provides a measure of steady-state LG where $LG = -V_{\text{r}}/V_{\text{d}}$. For a CPAP drop to be used to calculate LG, minute ventilation had to be significantly reduced from the eupneic level for the last 60 sec of the CPAP drop and no arousals could occur during this interval. All drops that met the criteria were spliced (to include the last 60 sec of the drop and 3 min following return to the therapeutic level), then normalized and ensemble averaged to produce a mean ventilation trace. This ensemble-averaged trace was then input to
a well-established minimal model of the ventilatory control system, to determine three characteristic parameters: the steady-state LG, the time constant of the ventilatory control system, and a delay (e.g., between the lungs and chemoreceptors). These parameters were identified for each subject using the System Identification Toolbox in MATLAB.

The components of steady-state LG, namely controller gain (ventilatory sensitivity to CO2) and plant gain (change in end-tidal CO2 for a given change in ventilation), were also determined as detailed previously. Briefly, plant gain (ΔPETCO2/ΔVET) was calculated based on the slope of the metabolic hyperbola and controller gain was subsequently deduced by dividing LG by plant gain (rearranging the equation; LG = controller × plant gain).

**Upper Airway Gain/Responsiveness**

The responsiveness of the upper airway muscles, referred to as the upper airway gain (UAG), was measured as the ratio of the amount that ventilation increases across the drop (V_uag) to the amount that ventilatory drive rises during the drop (V_r). This represents the ability of the airway to stiffen/dilate in response to the increase in drive (V_r), the subject activates his or her upper airway muscles and partially reopens the airway, allowing for ventilation to recover slightly (V_uag: determined by subtracting the mean ventilation on the last three breaths [open circles] of the drop from the mean ventilation of breaths two and three of the drop [circled]). The ratio of the compensatory increase in ventilation (V_uag) to the increase in ventilatory drive (V_r) across the drop provides a measure of neuromuscular compensation (V_uag/V_r), which we refer to as the upper airway gain (UAG). The breaths (two to three) following the reduction in CPAP were used to calculate the pharyngeal collapsibility or (see text for details) – the inset shows how the breaths from the current drop [circled] are placed on a graph of ventilation vs. mask pressure in order to calculate. Finally, if an arousal occurs during a drop, we quantify the arousal threshold as the level of ventilatory drive immediately preceding the arousal. However, in the example shown, there was no EEG arousal and thus this drop could not be used to determine arousal threshold.
to increases in ventilatory drive. In order to calculate the UAG, only CPAP drops in which no arousal occurred were used. $V_{\text{uag}}$ was calculated by subtracting the mean ventilation on the last three breaths of the drop from the eupneic ventilation of breaths two and three of the drop. $V_u$ was calculated by subtracting the mean ventilation of the first two breaths of the ventilatory overshoot (after CPAP was returned to the holding pressure) from the eupneic ventilation on optimum CPAP. The UAG is therefore $V_{\text{uag}}/V_u$, where a positive value indicates compensation, i.e., increased ventilatory drive, leads to a partial recovery of ventilation. By contrast, values near zero or negative values (i.e., no change or a further reduction in ventilation despite increased drive) indicate an inability to compensate.

### Passive Anatomy/Collapsibility

The passive anatomy, or pharyngeal collapsibility, was quantified by the ventilation on zero CPAP ($V_0$) when the upper airway muscles are inactive or passive. $V_0$ is determined by plotting mask pressure against ventilation for the third and fourth breaths of all CPAP drops throughout the night. These data points are then fit with a straight line (using linear regression) and $V_0$ is the $y$-intercept. A high ventilation value on zero CPAP indicates a good anatomy (i.e. resistant to airway collapse), whereas a low number indicates a poor anatomy (i.e. highly collapsible airway), because the subject is not able to achieve much ventilation at zero CPAP.

### Arousal Threshold

The arousal threshold was quantified as the ventilatory drive preceding arousal, defined as $>3$ sec of an abrupt increase in EEG frequency. Using a dynamic model of the ventilatory control system, the observed changes in ventilation that occur during the CPAP drops were transformed into a ventilatory drive based on a transfer function model with a steady-state LG, time constant and delay (measured during the drops from which LG was estimated). A ventilatory drive signal was then calculated for every CPAP drop. Once ventilatory drive was known, the arousal threshold could be determined from those CPAP drops in which an arousal occurred (see supplemental material for additional details).

### Statistical Analysis

Either independent samples $t$-tests or Mann–Whitney U tests were used to assess the effects of aging as appropriate and were performed using SigmaPlot (Systat Software, CA). $P \leq 0.05$ was considered significant. Values are presented as means ± standard error of the mean or medians [interquartile range] as appropriate.

### RESULTS

Subject demographics are shown in Table 1. By design, there was no difference in sex and BMI (despite younger individuals being both taller and heavier) between the groups. Both the objective CPAP compliance (average nightly usage over the past 30 days) and therapeutic CPAP requirement used were also similar between groups. There were no differences in major sleep characteristics between groups (Table 2) or respiratory event frequency during the clinical PSG (Table 3). However, the overall mean event duration was shorter in the younger subjects ($26.8 \pm 1.3$ versus $32.6 \pm 2.8$ sec; $P < 0.05$), which was driven by shorter hypopnea durations in NREM (Table 3).

### Effect of Aging on the OSA Traits

The four traits were estimated from either independent samples $t$-tests or Mann–Whitney U tests were used to assess the effects of aging as appropriate and were performed using SigmaPlot (Systat Software, CA). $P \leq 0.05$ was considered significant. Values are presented as means ± standard error of the mean or medians [interquartile range] as appropriate.

### Table 2—Effect of aging on sleep disordered breathing

<table>
<thead>
<tr>
<th>Variable</th>
<th>Young (n = 10)</th>
<th>Old (n = 10)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Total AHI (events/h)</td>
<td>48.8 ± 9.3</td>
<td>43.0 ± 6.2</td>
</tr>
<tr>
<td>Total sleep time (min)</td>
<td>315.5 ± 14.4</td>
<td>322.6 ± 15.5</td>
</tr>
<tr>
<td>REM duration (min)</td>
<td>33.0 ± 8.2</td>
<td>38.3 ± 7.3</td>
</tr>
<tr>
<td>NREM duration (min)</td>
<td>284.8 ± 11.6</td>
<td>284.7 ± 12.3</td>
</tr>
<tr>
<td>% Sleep efficiency (TST/TIB)</td>
<td>81.5 ± 3.8</td>
<td>74.4 ± 4.3</td>
</tr>
<tr>
<td>% REM (TST)</td>
<td>9.8 ± 2.4</td>
<td>11.5 ± 2.1</td>
</tr>
<tr>
<td>% Stage 1 (TST)</td>
<td>44.7 ± 8.5</td>
<td>47.4 ± 7.3</td>
</tr>
<tr>
<td>% Stage 2 (TST)</td>
<td>44.3 ± 6.6</td>
<td>40.9 ± 6.1</td>
</tr>
<tr>
<td>% Stage 3 (TST)</td>
<td>0 [0-1.0]</td>
<td>0 [0-0]</td>
</tr>
<tr>
<td>% Stage 4 (TST)</td>
<td>0 [0-0.2]</td>
<td>0 [0-0]</td>
</tr>
<tr>
<td>Mean overnight SaO₂ (%)</td>
<td>94.6 ± 0.5</td>
<td>94.7 ± 0.7</td>
</tr>
<tr>
<td>Lowest SaO₂ (%)</td>
<td>79.7 ± 2.5</td>
<td>81.0 ± 2.3</td>
</tr>
<tr>
<td>Oxygen desaturation index (events/h)</td>
<td>40.9 ± 9.6</td>
<td>40.7 ± 10.7</td>
</tr>
<tr>
<td>Total arousal index (events/h)</td>
<td>47.2 ± 9.3</td>
<td>36.3 ± 7.9</td>
</tr>
<tr>
<td>Respiratory arousal without desaturation (events/h)</td>
<td>4.1 ± 0.7</td>
<td>2.5 ± 0.8</td>
</tr>
<tr>
<td>Respiratory arousal with desaturation (events/h)</td>
<td>19.5 [5.8-53.2]</td>
<td>17.0 [11.5-25.5]</td>
</tr>
<tr>
<td>Leg movement arousals (events/h)</td>
<td>0 [0-0.1]</td>
<td>0 [0-0.0]</td>
</tr>
<tr>
<td>Spontaneous arousal index (events/h)</td>
<td>14.9 ± 2.9</td>
<td>12.8 ± 2.1</td>
</tr>
<tr>
<td>Leg movements (events/h)</td>
<td>0 [0-0.2]</td>
<td>0 [0-7.6]</td>
</tr>
</tbody>
</table>

Group data from the clinical polysomnogram in the supine posture and in the absence of continuous positive airway pressure. Values are means ± standard error of the mean or medians [interquartile range]. There was no statistical difference in any of the sleep measures between the young and old groups. AHI, apnea-hypopnea index; NREM, non-rapid eye movement sleep; REM, rapid eye movement sleep; SaO₂, arterial blood oxygen saturation; TIB, time in bed; TST, total sleep time.

### Table 1—Effect of age on anthropometric data

<table>
<thead>
<tr>
<th>Variable</th>
<th>Young (n = 10)</th>
<th>Old (n = 10)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Age (y)</td>
<td>32.1 ± 1.8</td>
<td>64.7 ± 1.2</td>
</tr>
<tr>
<td>Sex (F/M)</td>
<td>8/2</td>
<td>7/3</td>
</tr>
<tr>
<td>Height (cm)</td>
<td>179.8 ± 3.9</td>
<td>169.3 ± 2.6</td>
</tr>
<tr>
<td>Weight (kg)</td>
<td>106.7 [99.0-113.0]</td>
<td>88.3 [77.5-105.3]</td>
</tr>
<tr>
<td>BMI (kg/m²)</td>
<td>34.9 ± 1.8</td>
<td>31.3 ± 2.0</td>
</tr>
<tr>
<td>CPAP requirement (cmH₂O)</td>
<td>11.4 ± 0.8</td>
<td>11.9 ± 1.1</td>
</tr>
<tr>
<td>CPAP compliance (h/night)</td>
<td>6.7 ± 0.4</td>
<td>6.6 ± 0.0</td>
</tr>
</tbody>
</table>

Values are means ± standard error of the mean. * Significant difference compared with the younger obstructive sleep apnea cohort. BMI, body mass index; CPAP, continuous positive airway pressure; F, female; M, male.
subjects, respectively. The percentage of drops that were used to estimate LG and UAG (i.e., drops that did not end prematurely in an arousal with awakening) were similar in the young (16.0 ± 3.5%) and old group (19.1 ± 3.5%). There was no difference in arousal duration (13.1 ± 1.3 versus 15.9 ± 2.4 sec; P = not significant [NS]) or time to arousal from the start of the drop (44.5 ± 8.8 versus 52.2 ± 10.2 sec; P = NS) between groups.

Compared to younger individuals with OSA, older patients had a decreased minute ventilation on therapeutic CPAP or $V_{\text{capnea}}$ (8.2 ± 0.5 versus 6.1 ± 0.4 L/min; P < 0.01), a lower steady-state LG (5.0 ± 0.7 versus 2.9 ± 0.5; P < 0.05, Figure 2A), and a shorter time constant (81.3 ± 16.4 versus 45.5 ± 5.0 sec; P = 0.05) but no difference in circulation delay (8.0 ± 1.8 versus 8.2 ± 1.5 sec). The lower LG was primarily driven by a lower controller gain (0.70 ± 0.11 versus 0.36 ± 0.06 L/min/mmHg; P < 0.05, Figure 2B), as plant gain (Figure 2C) was similar between groups (7.47 ± 0.49 versus 8.55 ± 0.63 mmHg/L/min). Linear regression using pooled data demonstrated that both LG and UAG (i.e., drops that did not end prematurely in an arousal with awakening) were negatively correlated with NREM respiratory event duration (P < 0.05, Figure 3).

The effect of age on the remaining OSA traits is illustrated in Figure 4. $V_{\text{t}}$ was significantly lower in the older subjects (3.4 ± 0.9 versus 1.5 ± 0.7 L/min; P = 0.05), indicating that the airway becomes significantly more collapsible with age, whereas UAG (P = 0.9) and the arousal threshold (P = 0.16) were similar across age groups.

**DISCUSSION**

The major finding of our study was that among patients with OSA, the collapsibility of the pharyngeal airway worsens with aging, whereas the sensitivity of the ventilatory control system (i.e., LG) and the minute ventilation on therapeutic CPAP (i.e., $V_{\text{capnea}}$ or ventilatory demand) decreases. Our findings suggest that OSA in older adults is a unique phenotype due primarily to a worsening of the upper airway anatomy/collapsibility. This effect, however, is mitigated by a reduced ventilatory demand and feedback control sensitivity with age. By contrast, the phenotype in younger adults is one in which the airway is less collapsible, but a higher LG and greater ventilatory demand are dominant traits likely to contribute to the pathogenesis of OSA.

**Changes in OSA Traits with Age**

**Anatomy/Collapsibility**

In the current study, we found that the upper airway collapsibility ($V_{\text{t}}$) was worse in the older group. This result is consistent with a previous study that demonstrated in a large cohort of patients with OSA that age, independent of sex and BMI, was a significant predictor of pharyngeal collapsibility.22 Furthermore, worsening collapsibility is also found throughout life in healthy individuals, either when comparing children to adults,12 or with increasing age in adulthood.11 A number of studies suggest possible mechanisms for the age-related increase in pharyngeal collapsibility. Martin et al.31 measured upper airway caliber using acoustic reflection and found that all upper airway dimensions, except at the oropharyngeal junction, decreased modestly with age. Reduced airway caliber may be caused by the increased deposition of parapharyngeal fat in older individuals, either when comparing children to adults,12 or with increasing age in adulthood.11

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**Table 3—Effect of aging on NREM and REM sleep disordered breathing events and durations**

<table>
<thead>
<tr>
<th>Sleep stage</th>
<th>Young</th>
<th>Old</th>
</tr>
</thead>
<tbody>
<tr>
<td>Overall AHI</td>
<td>45.8 ± 9.4</td>
<td>40.8 ± 6.8</td>
</tr>
<tr>
<td>Central apneas</td>
<td>0 [0-0.3]</td>
<td>0.5 [0-1.4]</td>
</tr>
<tr>
<td>Obstructive apneas</td>
<td>1.3 [0-5.8]</td>
<td>0.9 [0-2.5-6]</td>
</tr>
<tr>
<td>Mixed apneas</td>
<td>0 [0-0.4]</td>
<td>0.1 [0-1.2]</td>
</tr>
<tr>
<td>Hypopneas</td>
<td>41.8 ± 8.8</td>
<td>35.8 ± 6.3</td>
</tr>
<tr>
<td>Overall AHI</td>
<td>43.5 ± 10.1</td>
<td>37.4 ± 6.9</td>
</tr>
<tr>
<td>Central apneas</td>
<td>0 [0-1.0]</td>
<td>0 [0-0.2]</td>
</tr>
<tr>
<td>Obstructive apneas</td>
<td>0 [0-10.1]</td>
<td>1.7 [0-6.5]</td>
</tr>
<tr>
<td>Mixed apneas</td>
<td>0 [0-0]</td>
<td>0 [0-0]</td>
</tr>
<tr>
<td>Hypopneas</td>
<td>35.1 ± 8.1</td>
<td>30.8 ± 6.2</td>
</tr>
</tbody>
</table>

Data represent medians [interquartile ranges] or means ± standard error of the mean. *Significant difference between young and old subjects with obstructive sleep apnea. AHI, apnea/hypopnea index; NREM, nonrapid eye movement; REM, rapid eye movement.

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**Figure 2—Effect of aging on loop gain and its components, controller and plant gain. The loop gain magnitude was approximately 50% (43% reduction) lower in the older subjects compared to the young subjects with OSA (A). The reduction in loop gain was driven by reductions in controller gain (B) with aging, as plant gain (C) remained unchanged. *P < 0.05.**

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**Sleep Apnea Phenotypes are Age Dependant—Edwards et al.**
may reduce the caliber of the upper airway and thus increase its propensity toward collapse. A recent study in nonobese individuals with OSA demonstrated that age was positively correlated with the amount of fluid shifting rostrally overnight.24 The authors argued that this finding may be caused by a more sedentary lifestyle in older adults, which can contribute to a greater amount of fluid accumulation in the legs during the day. The effect of age on other factors that increase pharyngeal collapsibility, such as increases in surface tension of the upper airway25 or decreases in lung volume tethering effects,26 may also be important and thus warrant investigation.

Loop Gain

Given the observations that aging is associated with an increased number of central apneas,27 oscillatory breathing,28 and with Cheyne-Stokes respiration in those with heart failure,29 we suspected that the ventilatory control system may become more sensitive with age. In fact, the current work shows that the steady-state LG decreases with aging in individuals with OSA. The longer respiratory events observed in older patients with OSA30 are also consistent with a less sensitive control system; indeed, our data confirm that the increase in event duration is associated with the decrease in LG with aging. Furthermore, a lowered LG with age is consistent with data in healthy subjects13; this relationship is likely driven by the known reduction in the ventilatory sensitivities to both oxygen and carbon dioxide with age.31 The current study confirms this finding by demonstrating that the aging-induced reduction in LG is driven solely via the decreases in controller gain, as plant gain was not different between groups. Overall, the available evidence suggests that the aging process leads to desensitization of the ventilatory control system.

Upper Airway Responsiveness

There is some evidence to suggest that aging attenuates the response of the genioglossus muscle (a major pharyngeal dilator muscle) to pharyngeal negative pressure stimuli15 and hypoxia12; however, these studies were conducted in healthy subjects during wakefulness. Thus, we do not know if (1) these deficits carry over into sleep, (2) are relevant in patients with OSA, and (3) whether reduced muscle responses that occur with aging translate into impairments in airflow. Interestingly, Patil et al.33 found no age-related change in the dynamic responses to upper airway obstruction (sometimes referred to as active Pcrit) during sleep in patients with OSA, a finding analogous to our observation that UAG was not altered with age.

Arousal Threshold

As several studies in older individuals have shown an increased number of spontaneous arousals during sleep,14 older adults might be expected to have a lower arousal threshold compared to younger individuals. In the current study we found no difference in the arousal threshold with age, a finding that is consistent with a cohort of healthy subjects,11 even when matched for BMI. Thus, the available data suggest that any effect that aging has on the arousal threshold appears negligible.

Are the Physiological Causes of OSA Different in Older Adults?

A major strength of the current work is that four physiological traits known to contribute to OSA were assessed simultaneously. To provide a detailed assessment of whether OSA might be caused by different mechanisms (or their interactions) in older compared to young individuals, we input the mean measurements of each trait into our previously published model (Figure 5).3 Ventilatory drive is represented on the x-axis and ventilation on the y-axis. The black circle represents the resting ventilation (V_{awake}) on therapeutic CPAP (e.g., 8.2 L/min for young subjects; panel A), which is equal to resting ventilatory drive (i.e., when the airway is fully patent). The slope of the black solid line is the reciprocal of the calculated LG, which shows how ventilatory drive increases as ventilation is reduced.
The gray dot represents the ventilatory drive (i.e., UAG). The point of intersection between the LG and UAG lines is the predicted steady-state ventilation when the ventilatory drive has increased. The gray dashed line represents the ventilatory drive threshold that when reached causes an arousal from sleep (i.e., arousal threshold). If the predicted steady-state ventilation is to the left of the arousal threshold, then the model predicts that breathing would remain stable (i.e., no OSA) because a mutually agreeable ventilation and ventilatory drive have been achieved at a ventilatory drive that is below the arousal threshold. However, if the steady-state point lands to the right of the arousal threshold line, then arousal occurs before stable breathing can be achieved as described below.

Figure 5A demonstrates that young subjects asleep on CPAP have a high resting ventilatory drive or V_eupnea. When CPAP is removed, the airway partially collapses and ventilation falls to 3.4 L/min. However, their passive anatomy would be considered quite good based on similarity to previous data in healthy subjects (mean ± standard deviation V_T in three control subjects = 3.0 ± 1.7 L/min, data from Wellman et al.8). As ventilation and ventilatory drive increase in response to this partial airway collapse in an effort to reach the intersection with the LG line, subjects hit their arousal threshold and arouse from sleep. As they fall asleep again, the airway partially collapses and the cycle repeats. Figure 5A suggests that a high resting ventilatory drive and high LG (relative to older adults) play a contributing role in the pathogenesis of OSA in young adults.

If young subjects were to have a V_eupnea and LG similar to older adults, then the model would predict that the intersection of the LG and UAG line would occur in the stable region and they would not have OSA (Figure 5C). It follows that if both V_eupnea and LG were the only factors that declined with age, then this effect should be protective against the predisposition to develop OSA. By contrast, we found that the passive anatomy worsens with age and we propose this is the predominant reason why older individuals develop OSA (Figure 5B). If older individuals had a passive anatomy that was similar to younger individuals, then we would predict that they would be less likely to develop OSA (Figure 5D). Thus, our evidence suggests that young and old people have OSA for different reasons.

The concept that OSAs is a different phenotype in older adults has also been suggested by studies that have shown strong associations between OSA and cardiovascular sequelae or neurocognitive impairment in middle-aged populations but not in older individuals. The milder clinical impact of OSA in older adults may be because of smaller ventilatory and cardiovascular responses to respiratory events/arousals compared to younger individuals. For example, older individuals who have been shown to produce less negative esophageal pressure during respiratory events than younger individuals may have reduced cardiac wall stress/tension (reflecting lower transmural pressure).30 If the characteristics of this older OSA phenotype is not simply a survivor effect (discussed in Limitations), then we speculate that it may contribute to the attenuated cardiovascular and neurocognitive sequelae in older adults, thus supporting the concept of redefining OSA based on underlying mechanism rather than simply focusing on AHI.

Role of Ventilatory Demand (V_eupnea) in the Pathogenesis of OSA
Ventilatory demand (V_eupnea) is not typically considered a physiological trait; however, the current study illustrates that lowering V_eupnea is one possible way to achieve stable breathing and resolve OSA (Figure 5C). Theoretically, lowering V_eupnea by 1 L/min has the same effect as improving the passive anatomy (V_T) by 1 L/min. That is, if a patient can only achieve a maximum ventilation of 5 L/min (see intersection of UAG and arousal threshold lines in Figure 5A) without arousing from sleep, then lowering V_eupnea to this level provides the possibility of stable breathing. V_eupnea can be lowered by either reducing metabolic rate or altering the characteristics of the ventilatory controller (i.e., reducing the slope of the ventilatory response to carbon dioxide or shifting this curve to the right). Our data suggest that the reduced V_eupnea observed in the older group is due to the combined effect of (1) reduced chemosensitivity (controller gain) and (2) a lowered metabolic production of carbon dioxide (compare 277 ± 24 versus 169 ± 16 mL/min; P < 0.01), which remained significantly different when accounting for differences in height and weight between age groups. Clearly more
Evidence is needed to confirm the role that \( V_{\text{eupnea}} \) plays in the pathogenesis of OSA, but if \( V_{\text{eupnea}} \) can be considered as a fifth trait, then we now have another potential therapeutic target to treat OSA.

**Limitations**

In addition to the possible limitations associated with our technique,\(^8\) there are several limitations that need to be considered when interpreting our findings. First, the small sample size in the current study may have meant that some of our comparisons were underpowered. Based on the results from the current study, we would need to study 70 young and 70 old subjects to determine definitively whether there was a reduced arousal threshold with age—which suggests that the true difference, if real, is small. Such a large study is clearly difficult to achieve in an intensive physiology laboratory.
Second, the cross-sectional nature of our study limits our ability draw firm conclusions as to whether the phenotypes are likely to change over time, or if the observed age-related differences were related to a selection bias. For example, it is plausible that the younger patients with OSA may not survive long enough to become old patients, and that the older group examined in the current study represents a specific survivor cohort in which their phenotype was protective; thus, it may not reflect an aging phenomenon per se as the older group may have had the same phenotype when they were younger. Third, it is possible that differences in the duration of exposure to CPAP (i.e., how long patients had been using CPAP) may have influenced our measurements of the four traits. Although we did not document the treatment duration in our study, studies that have assessed the effect of CPAP treatment on the phenotype traits have shown that 1 mo of CPAP therapy reduced controller gain (and therefore loop gain) back to the same levels measured in healthy controls, and lowered the arousal threshold but did not alter the upper airway muscle responsiveness. Such findings suggest that 1 mo of effective treatment is sufficient to reverse the consequences of disease and allows an individual’s intrinsic physiology to be assessed. Given that our patients had at least 2 mo of documented CPAP usage, and that the average nightly usage (over the past 30 days) was not different between groups, we believe that any difference in duration of CPAP exposure between the groups is unlikely to affect our measurements (i.e., we are comparing the intrinsic physiology in both groups). Last, we did not study any subjects without OSA, making it difficult to demonstrate conclusively that the changes in the traits are caused by age alone. However, our reported changes in the traits in patients with OSA are consistent with existing data in healthy subjects. Nonetheless, until many of these limitations are addressed, we will not have the complete answer as to how the phenotypic traits are altered with age. Ultimately our findings need to be repeated in larger (ideally longitudinal) studies involving both patients with OSA (treated and untreated) and those without OSA.

CONCLUSIONS

Our data support the emerging concept that OSA may be a different phenotype in young versus old individuals. Young individuals with OSA have relatively good anatomy, but a higher respiratory drive and higher loop gain (LG) predispose them to OSA. Although the reduction in ventilatory drive and LG with age should protect against OSA, any reduction in the predisposition toward OSA is offset by worsening anatomy with age. Future research should focus on measuring physiological traits in large cohorts of subjects (ideally followed longitudinally) to assess definitively how aging alters the factors causing OSA and its sequelae.

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DISCLOSURE STATEMENT

This was not an industry-sponsored study. Dr. Wellman is a consultant for Philips Respironics, SOVA Pharmaceuticals and Apex Medical. Dr. Owens consults for Apex Medical, Apnicure and Philips Respironics. Dr. White was the chief medical officer for Philips Respironics until 12/31/12 but is now the chief scientific officer for Apnicure Inc as of January 2013. Dr. Malhotra was a consultant for Philips Respironics, SHC, SGS, Apex Medical, Pfizer, Apnicure, but has relinquished all outside personal income since May 2012. The other authors have indicated no financial conflicts of interest.

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SUPPLEMENTAL METHODS AND RESULTS

Measuring the Passive Anatomy/Collapsibility: Comparison with \( P_{\text{crit}} \)

The passive anatomy or pharyngeal collapsibility was quantified by the ventilation on zero CPAP (\( V_0 \)) when the upper airway muscles are inactive or passive. \( V_0 \) is determined by plotting mask pressure against ventilation for the second and third breaths of all CPAP drops throughout the night. These data points are then fit with a straight line (using linear regression) and \( V_0 \) is the y-intercept. A high ventilation value on zero CPAP indicates a good anatomy (i.e. resistant to airway collapse), whereas a low number indicates a poor anatomy (i.e. a highly collapsible airway), as the subject is not able to achieve much ventilation at zero CPAP. It is worth noting that this technique is analogous to measuring the ‘passive’ critical pharyngeal closing pressure (\( P_{\text{crit}} \)), which plots peak flow (instead of ventilation) from the third through fifth flow-limited breaths after a pressure drop against mask pressure and fits these points with a straight line. The x-intercept of this line (zero flow crossing) is then taken as the \( P_{\text{crit}} \). From our CPAP drops we were also able to determine a \( P_{\text{crit}} \) for each subject. Similar to our analysis using \( V_0 \), we found that the \( P_{\text{crit}} \) was less collapsible in the younger group (compare -1.0 ± 1.5 versus 0.8 ± 0.8 cmH2O) and that \( P_{\text{crit}} \) and \( V_0 \) were strongly correlated (\( r^2 = 0.60 \), \( P < 0.001 \)).

Measuring the Arousal Threshold

The arousal threshold was quantified as the ventilatory drive preceding arousal, defined as >3 sec of an abrupt increase in electroencephalographic frequency. Using a dynamic model of the ventilatory control system, the observed changes in ventilation that occur during the CPAP drops were transformed into a ventilatory drive based on a transfer function model with a steady-state LG, time constant, and delay (measured during the drops from which LG was estimated). A ventilatory drive signal is then calculated for every CPAP drop. When ventilatory drive is known, the arousal threshold can be determined from those CPAP drops in which an arousal occurred. A schematic of how the arousal threshold is calculated is shown in Figure S1.

REFERENCES